

Overcoming biological barriers to in vivo efficacy of antisense oligonucleotides

Paul J. White^{1,*}, Frank Anastasopoulos^{1,2}, Colin W. Pouton¹ and Ben J. Boyd¹

Antisense oligonucleotides as a therapeutic platform have been slow to progress since the approval of the first antisense drug in 1998. Recently, there have been several examples of convincing antisense interventions in animal models and promising clinical trial data. This review considers the factors determining the success of antisense oligonucleotides as therapeutic agents. In order to produce target knockdown after systemic delivery, antisense oligonucleotides must avoid nuclease degradation, reticuloendothelial-system uptake and rapid renal excretion, and extravasate to the target cell type outside the vasculature. They then must enter the target cell, and escape the endosome-lysosome pathway so as to be free to interact with the target mRNA. We consider the significance of these limiting factors based on the literature and our own experience using systemic administration of antisense oligonucleotides.

It has been recognised for many years that antisense oligonucleotides – short single-stranded nucleic acid sequences that inhibit target gene expression via sequence-specific, Watson–Crick base-pair hybridisation to sense mRNA – can be employed to selectively reduce the expression of disease-related proteins in vivo, and consequently to improve disease phenotypes. A large number of biotechnology companies have emerged in that time with a view to translating the promise of ‘antisense’ in cell culture and animal models to successful pharmaceutical products. Target proteins as varied as the low-density lipoprotein (LDL)–

cholesterol component apolipoprotein B100 (Refs 1, 2, 3), the skeletal muscle protein dystrophin (Refs 4, 5, 6), hepatitis C viral proteins (Ref. 7) and intracellular signalling molecules (often proto-oncogenes such as MYC; Refs 8, 9, 10) have all been shown to be ‘knocked down’ in animal models using antisense oligonucleotides and tested in clinical trials. Since the approval in 1998 of the first antisense drug, fomivirsen (Vitravene[®]; Refs 11, 12), which targets a cytomegalovirus mRNA, there has been a notable dearth of subsequent approvals for therapeutics of this type, due to a variety of factors preventing promising

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¹Monash Institute of Pharmaceutical Sciences, Monash University, Parkville, Victoria 3052, Australia.

²Clinical Vision Research Australia, Victorian College of Optometry, Carlton, Victoria 3053, Australia.

*Corresponding author: Paul J. White, Medicinal Chemistry and Drug Action, Monash Institute of Pharmaceutical Sciences, Monash University, 381 Royal Parade, Parkville, Victoria 3052, Australia. Tel: +613 99039074; Fax: +613 99039638; E-mail: paul.white@pharm.monash.edu.au

antisense candidates from reaching the clinic. Recently, however, there have been some positive clinical trial data from Isis Pharmaceuticals (Refs 1, 13), and several high-impact publications demonstrating excellent outcomes of antisense therapy in animal models of human disease (Refs 5, 14, 15, 16). Thus, it is timely to review the pharmaceutical science underlying the *in vivo* effects of antisense oligonucleotides. We focus here on the nature of the biological barriers to *in vivo* knockdown and strategies that have already overcome each barrier or may do so in the future, and then analyse the efficacy and potency of antisense therapeutics after intravenous administration.

Natural deoxyribonucleotides are not used as antisense oligonucleotides *in vivo* because of stability and delivery problems, and several chemical modifications have been introduced over the past decade to improve the efficiency of antisense therapeutics. The pharmaceutical chemistry of antisense oligonucleotides is reviewed elsewhere (Refs 17, 18, 19, 20, 21). The modifications considered in this article include: (1) first-generation phosphorothioate (PS) DNA antisense; (2) second-generation 2'-O-alkyl (particularly 2'-O-methoxyethyl; MOE) 'gapmer' chimaeric DNA-RNA antisense (Ref. 21); (3) phosphorodiamidate morpholino (PMO) antisense (Ref. 22); (4) peptide nucleic acid (PNA) (Ref. 23); and (5) locked nucleic acid (LNA) antisense (Refs 18, 24). These modifications and others have achieved the goal of producing nuclease-resistant antisense agents that retain high efficacy *in vitro*. 2'-O-modification and LNA chemistries do not support RNase H activity, and oligonucleotides containing these chemistries therefore require regions free of 2'-modification to recruit this high-efficiency silencing mechanism. Monia and colleagues demonstrated that a region containing five or more 2'-deoxy nucleotides was required for RNase H activity (Ref. 25). A major innovation allowing the benefits of MOE, 2'-O-methyl (OMe) and LNA chemistries to be realised without the loss of efficacy has thus been the use of gapmer strategies (Refs 25, 26, 27, 28) in which central regions of the oligonucleotide consisting of nucleotides whose chemistry supports RNase H activity – that is, unmodified phosphodiester (PO) internucleoside linkages (PO or PS) – are flanked by 2'-modified regions

(eg. MOE-PS-MOE). PMO oligonucleotides differ from the other modifications described above in that these agents are designed to work via steric inhibition of translation rather than degradation of mRNA transcripts.

This review focuses mainly on the barriers to efficacy of second- and third-generation antisense oligonucleotides *in vivo*, with a view to informing the use of antisense as both a research tool in animal models and a therapeutic platform in humans. Much of the research described herein is from animal studies that have revealed insights into antisense mechanisms; where informative human data are available, these have also been included.

General pharmacokinetic properties of antisense oligonucleotides

Antisense oligonucleotides exhibit predictable pharmacokinetic properties given their size and charge. They can exist as free molecules within the plasma or exhibit strong plasma protein binding depending on sequence and modification. Antisense oligonucleotides almost universally exhibit biphasic plasma concentration-time profiles, usually with a rapid initial decrease in plasma concentration within the first hour after intravenous injection in mice (Ref. 29), rats (Ref. 30) and humans (Ref. 29) ($t_{1/2\alpha}$ of around 3–30 min), even for nuclease-stable antisense (Refs 31, 32), and a slower second phase of clearance over the next 24 h ($t_{1/2\beta}$) (Refs 30, 33). In humans, a similar pharmacokinetic profile is observed for PS oligonucleotides (Refs 33, 34, 35). A cross-species comparison for ISIS 301012 found only small differences between the pharmacokinetic properties of the drug in mice, rats, monkeys and humans (Ref. 29). For nuclease-stable oligonucleotides, the biphasic nature of the fall in plasma concentration represents a combination of renal excretion, tissue distribution and tissue clearance, considered in the following sections.

Tissue distribution

The kidney and liver are the predominant destinations for antisense oligonucleotides. More than 80% of the antisense oligonucleotide detected in tissues after intravenous administration is found in these two organs, and these observations are valid for both charged (Ref. 31) and uncharged (Ref. 30) antisense oligonucleotides, and also after oral

(Refs 32, 36) or intradermal (Ref. 36) delivery. When the spleen is included in the analysis, the proportion of dose within these tissues rises above 90% in many cases.

Table 1 shows representative examples of tissue distribution for oligonucleotides of varying chemistries. The major determinants of tissue distribution remain unclear to some extent, but blood flow, specific cellular uptake (e.g. reticuloendothelial function) and preference for organs with fenestrated vascular endothelia all appear to be relevant factors, as considered further in the next section. The liver and kidney receive large proportions of cardiac output, and these organs accumulate significant proportions of an administered oligonucleotide dose, with

the kidney predominant for all chemical modifications other than PS (Table 1). However, oligonucleotide distribution is not always directly proportional to the blood flow to that organ. Collectively, skeletal muscle receives >20% of cardiac output in mice (Ref. 37) and rats (Ref. 38), yet retains <5% of oligonucleotide across a variety of modification types and experimental protocols (Table 1), and the heart and gastrointestinal tract also show discordance between the proportion of cardiac output received and the proportion of oligonucleotide they contain (Table 1). Thus, there is preferential distribution of oligonucleotide to liver, kidney and spleen (and bone marrow) at the expense of other tissues.

Table 1. Tissue distribution of the major classes of modified antisense oligonucleotides after systemic administration^a

Modifi- cation (Ref.)	Dose (mg/ kg)	Time of tissue collection (min)	Kidney	Liver	Spleen	Heart	Intestine	Skeletal muscle
Mouse								
PS (Ref. 39)	0.8	90	20 ^c	180	20	<5	NR	NR
MOE gapmer (Ref. 40)	5	1440	90 ^c	20	20	<5	<5	NR
LNA (Ref. 72)	6	1440	175 ^d	15	<10	<5	5-10	<1
Rat								
PS (Ref. 44)	0.04	120	13 ^c	15	5	<2	<2	<1
LNA mixmer (Ref. 58)	0.01	120	15 ^c	40	30	<2	<2	<2
PMO (Ref. 48)	15 ^b	1440	10 ^e	20	10	5	NR	NR
PNA (Ref. 30)	5	120	180 ^d	10	5	5	NR	NR
Monkey								
MOE gapmer (Ref. 31)	10	1440	300 ^d	25	<10	NR	<5	NR

^aFrom each article, we extracted the following information: the dose used in animals (^bdaily injections for 5 days), the time of tissue collection and the concentration of drug in each tissue. To allow comparison, we normalised the tissue concentration data to those of the kidney, which for the majority of studies contained the greatest concentration of oligonucleotide. Values are approximates that we calculated from figures within the cited articles, expressed as % dose^c, concentration^d (μg/g) or micromolar concentration^e. Abbreviations: LNA, locked nucleic acid; MOE, 2'-O-methoxyethyl; NR, not reported; PMO, phosphorodiamidate morpholino; PS, phosphorothioate.

Tissue clearance of oligonucleotide

The clearance of oligonucleotide from the liver, kidneys and spleen is slow, and due in large part to nuclease degradation. The tissue half-life of most nuclease-resistant oligonucleotides is extremely long, with reported values generally expressed in days rather than hours (Refs 39, 40). The rate of clearance, and resultant duration of action of the oligonucleotide, is dependent on the modification, with MOE oligonucleotides demonstrating tissue half-lives greater than 10 days across a number of tissues and across species (Ref. 40).

Barriers to efficacy of antisense therapeutics

Overview

In order to gain access to complementary mRNA species within tissues after systemic administration, antisense oligonucleotides must avoid nuclease degradation, reticuloendothelial system uptake and renal excretion, traverse the microvascular endothelium, cross target cell membranes and escape the endosome-lysosome system (Fig. 1). The combination of these barriers has contributed to the requirement for larger doses to be used in animal experiments and clinical trials, and thus greater class-related and drug-specific toxicity. The failure of antisense oligonucleotides in clinical trial has resulted from deficiencies of both efficacy and safety (Ref. 41). In many cases it has been difficult to measure target knockdown as an indicator of efficacy. For those cases where clinical efficacy has been lacking, it is often difficult to assign this to a failure of stability, delivery to the target cell type, uptake, endosomal escape, mRNA cleavage, or choice of the therapeutic target. For example, the development of GEM91 by Hybridon was halted when dose-limiting thrombocytopenia occurred in Phase II trial, but in any case the efficacy seen in Phase I trial (as indicated by levels of viraemia) was not replicated in the Phase II trial according to a press release (Ref. 42) – greater understanding of the fate and efficacy during the development of GEM91 may have prevented the failure or indicated that development should be halted at an earlier point. Where target knockdown can conveniently be correlated with disease outcomes, such as for ISIS301012 (Refs 1, 13), the close evaluation of

efficacy during each stage of development allows for more informed drug development.

Barrier 1: nuclease degradation

Studies using radiolabelled phosphodiester antisense oligonucleotides have shown that these agents are likely to have little utility in vivo because of rapid nuclease degradation (Refs 43, 44, 45), with <15% of intact drug detectable in rat plasma 20 min after dosing (Ref. 44). The major modified antisense chemistries have overcome this problem to a large extent. PS oligonucleotides (Ref. 43), MOE-PS-MOE gapmers, LNA oligonucleotides (Ref. 46) and LNA-DNA-LNA gapmers (Ref. 26) are stable in serum for extended periods, whereas OMe-PS-OMe gapmers show moderate serum stability in vivo (Ref. 47). A study using a gel-shift assay to detect degradation of PNA in rat tissue and urine samples after intravenous administration found no detectable degradation products (Ref. 30). PMO oligomers show good serum stability in rats after intravenous injection, as does the PMO portion but not the cell-penetrating peptide portion of PMO-cell-penetrating peptide conjugates (Ref. 48). The extent of modification is an important factor here, with fully modified PS being more stable than partially modified PO/PS sequences (Ref. 47).

Barrier 2: clearance from the blood by the kidney and reticuloendothelial system

Clearance via the kidney

The degree of renal excretion of antisense oligonucleotides varies widely depending on the chemical modification, dose and species. Unmodified oligonucleotides are rapidly metabolised and degradation products renally excreted (Ref. 26). PS oligonucleotides often display far lower rates of renal clearance; some PS sequences are able to avoid glomerular filtration by binding to plasma proteins such as albumin (Ref. 49). The degree of renal excretion has been reduced to a low level using PS antisense oligonucleotides selected for high plasma-protein-binding affinity; two antisense molecules that exhibited >90% plasma protein binding showed slow plasma clearance in monkeys, while an antisense with <80% plasma protein binding exhibited rapid plasma clearance (Ref. 31). This study also demonstrated

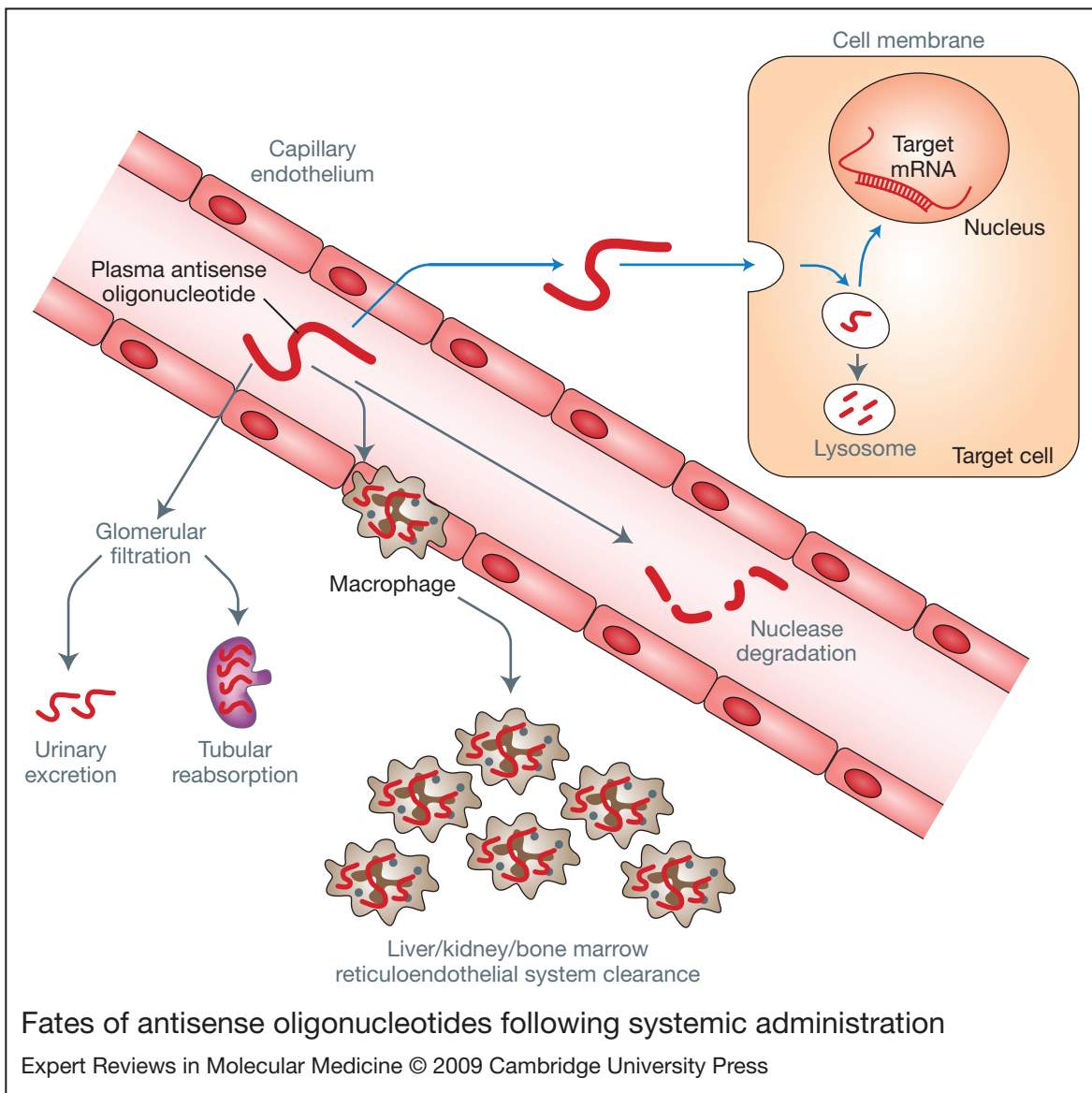


Figure 1. Fates of antisense oligonucleotides following systemic administration. (a) Successful gene silencing after systemic administration requires the movement of the antisense oligonucleotide from the blood into the interstitium, then into the target cell (nucleus) to reach the target mRNA (blue arrows). (b) However, there are several barriers and mechanisms to prevent successful knockdown (grey arrows and grey labels). Antisense oligonucleotides may be degraded in the blood, or removed by renal excretion or uptake by tissue macrophages. Antisense oligonucleotides may not reach their target cells because they are unable to escape across the vascular wall. Once in the interstitium, antisense oligonucleotides may be prevented from reaching their intracellular target (mRNA) by an inability to cross the cell membrane or escape the endosome-lysosome pathway.

that, in mice, the proportion of PS oligonucleotide excreted in the urine increased at doses >5 mg/kg, suggesting saturation of albumin binding. Furthermore, MOE gapmers with increasing proportion of phosphodiester internucleoside

linkages show increasingly greater renal excretion than those containing fully phosphorothioated central regions (Ref. 50). It is pertinent to emphasise that not all PS oligonucleotides share the property of low renal clearance: an early study

in humans found that a low dose (0.1 mg/kg) resulted in ~50% urinary excretion within 24 h in human immunodeficiency virus (HIV) patients (Ref. 33), possibly as a result of a sequence that exhibits low affinity for albumin. Nonetheless, PS oligonucleotides can be developed to exhibit low urinary excretion in humans: <10% of the administered dose of ISIS 104838 (Ref. 34) and ISIS 2302 was found in urine 24 h after intravenous dosing, and the low level of urinary excretion is retained in the MOE gapmer ISIS 301012 in humans (Ref. 29). Methodological differences may account for some of the variability in reported plasma levels and urinary excretion; for example isotope choice and placement can affect the quantitation of urinary excretion rates for radiolabelled drug (Ref. 39).

Non-PS oligonucleotides generally exhibit greater urinary excretion than PS oligonucleotides. Urinary excretion of OMe-PS-OMe gapmer oligonucleotides has been shown to be extensive (30–50%) over 72 h (Ref. 47), although this study employed a high dose, which may have increased the level of urinary excretion as discussed above. PNA oligomers appear to undergo rapid and extensive urinary clearance: in rats, >90% of a 5 mg/kg intravenous dose was recovered as parent drug in the urine (Ref. 30), although this characteristic may not hold for PNAs containing positively charged residues (Ref. 51). A comparison of LNA and PS oligonucleotide urinary excretion (Ref. 46) revealed far greater renal excretion of the LNA than the PS 30 min after intravenous injection in nude mice. Although the albumin-binding affinities for these modifications are often untested, it is possible to speculate that a lower affinity for albumin was responsible for the rapid urinary excretion of LNA oligonucleotides. For chemistries with low albumin-binding affinity, strategies that reduce renal excretion, including particle-based approaches, will be expected to increase the efficacy of the drug.

Uptake by cells within the kidney

The amount of drug retained within the kidney is of interest both from the perspective of targeting kidney disease and in relation to renal oligonucleotide toxicity. The mechanisms of uptake of antisense into proximal tubule epithelial cells (the major cellular location

for oligonucleotides within the kidney) (Refs 52, 53) are worth consideration, particularly given the differing importance of renal excretion for PS and non-PS oligomers described above. Proximal tubule epithelial function is important in renal oligonucleotide accumulation, as the use of cisplatin to disrupt this activity has been shown to decrease oligonucleotide concentration in the renal cortex (Ref. 54). For LNA, PNA and PMO oligonucleotides, the exposure of the proximal tubule epithelium to high concentrations of drug in the filtrate would be expected to result in significant uptake in this actively sampling cell type.

An interesting conceptual problem arises for PS oligonucleotides: given the extremely low levels in the urine for first- and second-generation oligonucleotides with high albumin-binding affinity, how do the proximal tubule cells gain access to the drug? Clearly, access is possible, in that the renal cortex usually contains >20% of an administered dose (Table 1), localised to granular structures within proximal tubule epithelial cells (Ref. 55). The answer appears to be that both basolateral uptake from the blood and tubular reabsorption from the filtrate contribute to PS uptake into proximal tubule epithelial cells (Refs 53, 56), with the latter predominant (Ref. 57). The ratio of Bowman's capsule to plasma concentration of ³⁵S-labelled PS oligonucleotide has been found to be low in rats (Ref. 53), indicating that filtration of these agents was limited to some extent. However, tubular reabsorption of PS oligonucleotide did 'account for the large amount of oligonucleotide found in the kidney after intravenous infusion' (Ref. 53). In isolated, perfused rat kidneys under nonfiltering conditions, PS oligonucleotide absorption from capillaries has been observed; furthermore, this absorption was reduced in the presence of polyanions (Ref. 49). The fraction absorbed from the capillaries constituted only a small fraction, however, of the total renal uptake in filtering conditions for PS oligonucleotides. One conclusion to be drawn from these data is that a small but significant amount of PS oligonucleotide (the unbound fraction in the albumin-oligonucleotide equilibrium) is, in fact, filtered and that efficient tubular reabsorption of this

filtered drug accounts for most of the MOE–PS–MOE gapmer in the renal cortex after intravenous administration.

Uptake by the reticuloendothelial system

The reticuloendothelial system, consisting of mononuclear leukocytes that circulate in the blood and enter tissues to become scavenging macrophages, appears to play an important role in the removal of antisense oligonucleotides from the blood. After systemic administration, high concentrations of PS, PO, LNA hybrid oligonucleotides and OMe oligonucleotide are found in bone marrow (Refs 44, 58, 59) (in particular in large nucleated cells within the red bone marrow; Ref. 60), within the spleen (Refs 40, 58) (in particular in the red pulp of the spleen; Ref. 60) and in resident macrophages (Kupffer cells) in the liver (Ref. 61). These findings suggest that macrophage-mediated uptake of oligonucleotide plays an important role in the tissue distribution of these agents. Within the liver, Kupffer and endothelial cells show high levels of PS oligonucleotide after intravenous injection: a study in rat liver showed that 80% of the total organ cellular PS oligonucleotide dose was located within these cells, whereas hepatocytes exhibited relatively poor uptake and, despite the larger number of hepatocytes, only 20% of the liver-associated oligonucleotide was found in this cell type (Ref. 60). Higher doses of oligonucleotide may be required to cause antisense inhibition in hepatocytes compared with Kupffer cells (Ref. 61). Uptake of PS oligonucleotides by cells of the reticuloendothelial system has been suggested to be dependent on 'scavenger receptor' binding. Nonspecific anionic inhibitors of scavenger receptors such as dextran sulphate impair hepatic and splenic uptake of PS oligonucleotide in a dose-dependent manner (Ref. 57). However, comparison of mice deficient in the predominant candidate scavenger receptor (SR-A) with wild-type mice shows either no difference or modestly reduced cellular uptake (Kupffer cells) of PS oligonucleotides (Ref. 62). The specific proteins responsible for cellular uptake in vivo across different cell types remain elusive.

A variety of delivery strategies have since been successful in avoiding or reducing uptake of antisense oligonucleotides by the

reticuloendothelial system. Cholesterol conjugation of PS oligonucleotide results in impressive targeting to the liver such that it contains about 80% of the administered dose, and a redistribution to endothelial cells and hepatocytes rather than Kupffer cells is observed (Ref. 63). However, uptake of liposomally encapsulated oligonucleotide by the reticuloendothelial system is enhanced compared with free oligonucleotide (Ref. 64). This altered disposition was used to advantage (Ref. 65) to deliver TNF- α antisense to macrophages in vivo. These studies demonstrate that shifting between a predominantly reticuloendothelial system and a predominantly hepatic parenchymal distribution is possible. What is still lacking in the literature is a reliable delivery system that results in avoidance of both reticuloendothelial system and hepatic uptake such that the concentration in other organs increases.

Barrier 3: extravasation in organs other than liver, kidney and spleen

One aspect of antisense oligonucleotide pharmacokinetic behaviour that is often ignored is the relative ability of these molecules to escape the vasculature. The microvascular endothelium, in organs other than the kidney and liver, consists of a cell monolayer with close intercellular connections, which excludes relatively large hydrophilic species such as antisense oligonucleotides as a result of their inability to partition across the lipid regions of the cellular membrane or to penetrate the tight junctions between the endothelial cells.

The importance of extravasation as a barrier to antisense efficacy has not been directly evaluated. The low concentration within lymph nodes in mice after intravenous injection of up to 100 mg/kg PS oligonucleotide observed previously (Ref. 39) suggests that extravasation might be a limiting factor for these agents. Other indirect evidence may be inferred from the lack of partitioning of antisense oligonucleotides into organs other than the liver, kidney and spleen, which have either fenestrated or sinusoidal endothelia. However, this argument may be countered by the fact that specific mechanisms described earlier (macrophage and renal proximal tubule epithelial uptake) may be largely responsible

for the high concentration of drug retained within these tissues.

For organs such as the heart, antisense strategies will require enormous efficacy from their therapeutic agents, as generally <5% of the systemically delivered dose reaches and/or is retained within these organs (Table 1). For tissues where the drug access is very poor, in particular the central nervous system, it appears very unlikely that systemically delivered antisense oligonucleotides will have a major role to play in future therapeutic strategies without delivery systems that enhance access to target cells. An exception might be made for PNAs, which have been demonstrated to reach and produce measurable antisense effects in the central nervous system (Ref. 66) after intraperitoneal administration – a finding attributed to an ability to partition across the blood–brain barrier due to lack of charge on the molecule. Tumours represent an atypical tissue type in many respects, including microvascular barrier function. Tumours are supplied by altered microvasculature, which allows for increased access to and retention of macromolecules (Ref. 67). In humans, PMO oligomers were found to reach significant concentrations within breast and prostate tumours after a single 90 mg dose, with tumour drug concentrations similar to *in vitro* knockdown IC₅₀ values (Ref. 8).

A theme that emerges when considering barriers to antisense efficacy *in vivo* is that successes in the antisense field appear to involve (1) choice of targets that play to the strengths of the pharmacokinetics and tissue distribution of antisense oligonucleotides, or (2) strategically using chemical modification or delivery strategies that alter pharmacokinetics or tissue distribution towards a favoured target.

Barrier 4: cellular uptake

The ability of antisense oligonucleotides to produce target knockdown is of course also dependent on the level of uptake into the target cell. An observation from animal studies is that, unlike cultured cells, several cell types *in vivo* take up oligonucleotide via a process that results in high nucleus to cytoplasm concentration ratios (Refs 60, 68). Keratinocytes avidly take up oligonucleotide in a manner that results in nuclear localisation after intradermal injection *in vivo* (Ref. 68) but not *in*

vitro (Ref. 69), and the same distribution pattern has been observed in freshly isolated gastric smooth muscle cells in the absence of transfection reagent (Ref. 70). It is clear that if sufficient antisense oligonucleotide can gain access to many cell types *in vivo*, there is a good chance for cellular uptake and successful target knockdown in that tissue. Furthermore, an *in vitro* study modelling the barriers to antisense efficacy found that intracellular trafficking and the affinity for target mRNA may be of greater significance than total cellular uptake (Ref. 71). Although promising, these results do not demonstrate that efficacy in a particular organ is assured when significant tissue drug concentrations are observed. For example, splice correction has been demonstrated using LNA oligonucleotides in liver and gastrointestinal tract but not in kidney – the organ where by far the greatest accumulation of drug occurred (Ref. 72). Delivery strategies that allow for cellular entry *per se* are not necessarily effective, but those that promote cellular entry in a manner that avoids subsequent endosome–lysosome trapping are likely to be very productive, as described in the next section. A greater understanding of cellular uptake mechanisms for free antisense oligonucleotide is important for continued development of antisense strategies.

Cell-penetrating peptides have been used to promote the cellular uptake of antisense oligonucleotides. Although these agents have shown great promise, and some *in vivo* efficacy has been demonstrated using conjugation with Tat from HIV (Refs 73, 74), it is not apparent at this stage that cell-penetrating peptides provide a robust system for cellular uptake of antisense oligonucleotides. Methods that produce cell-type-specific uptake of antisense oligonucleotides have long been sought, with little success. In this regard, the field of small interfering RNA (siRNA; RNA duplexes that cause silencing via RNA interference) has perhaps developed at a greater rate than that of antisense oligonucleotides (Ref. 75).

Barrier 5: endosomal escape and particulate strategies to enhance delivery of antisense oligonucleotides

The endosome–lysosome pathway is clearly a major limiting factor to access of the

oligonucleotide to mRNA. Cationic polymers and cationic liposomes have been used extensively in cell culture to allow antisense oligonucleotides to escape endosomes and gain access to target mRNA. However, the systemic administration of cationic particles and complexes, such as lipoplexes, leads to rapid uptake by macrophages (Ref. 65). Approaches using polyethyleneimine alone have been successful in models of inflammatory disease (Ref. 76). Moderate success has been reported with shielding of the polycation from the reticuloendothelial system facilitated by a surface coating of polyethyleneglycol (Ref. 77).

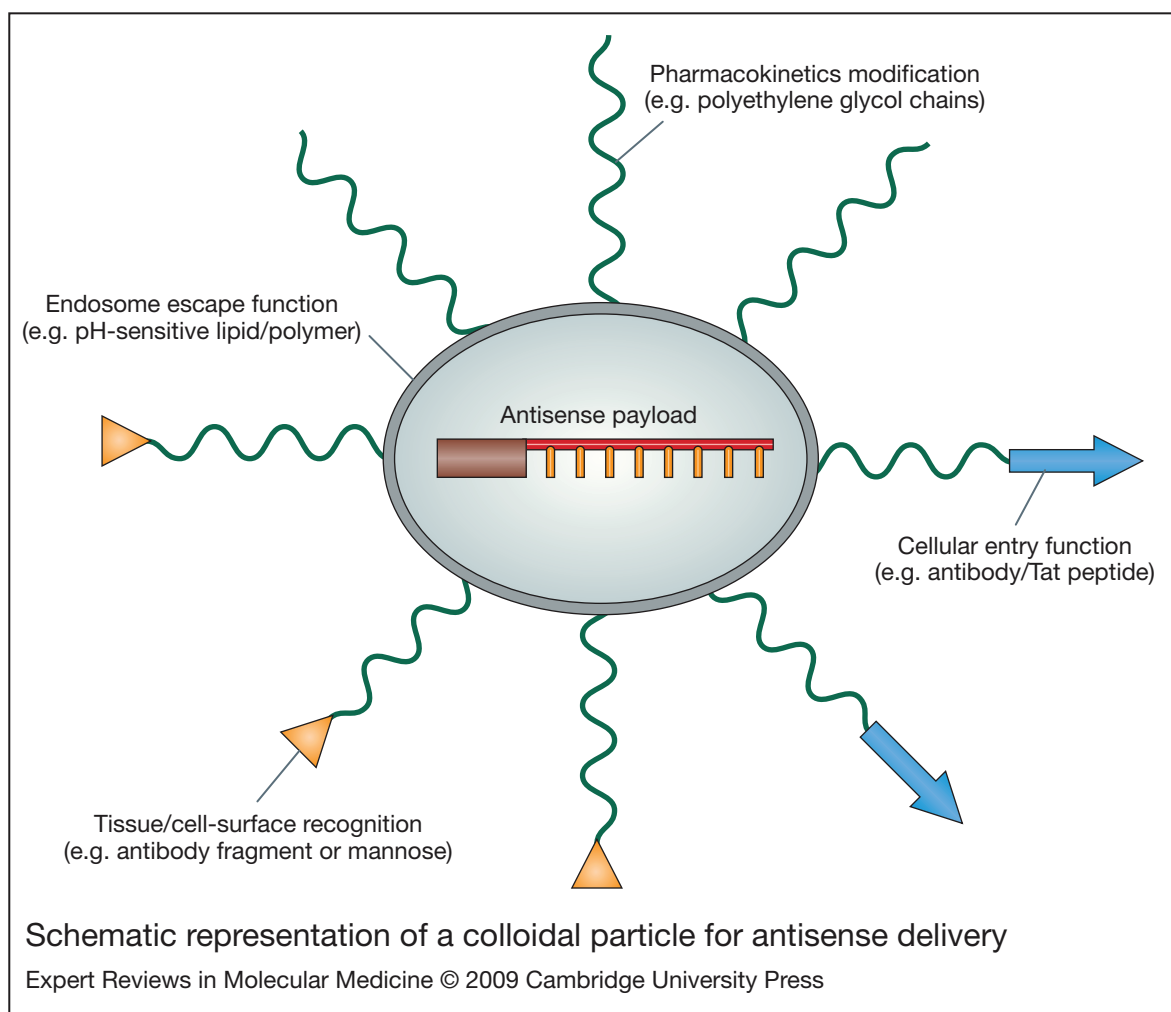
Future directions: overcoming barriers to antisense oligonucleotide

Attempts to overcome the biopharmaceutical barriers to systemic administration of antisense therapeutics have therefore developed towards rational design of multifunctional antisense oligonucleotide delivery systems – either as colloidal particles held together by electrostatic attraction or using medicinal chemistry advances to produce novel modified oligonucleotides. The goals in each case are to provide one or more of the following: improved pharmacokinetic profiles, and selective targeting to particular tissues through modification of the particle surface with ligands that allow targeting, cellular uptake and endosomal release. A schematic of such a colloidal construct is shown in Figure 2.

Polymer-based nanoparticles are a colloidal system that has received recent attention for delivery of antisense; of particular interest are particles prepared using biodegradable polymers such as poly(D,L-lactide-co-glycolide) (Ref. 78), which can be used to release therapeutic agent slowly as the polyester is degraded by hydrolysis. Chitosan, a cationic biopolymer that can be prepared in nanoparticle form, has also been shown to be useful for encapsulation and cellular uptake of antisense oligonucleotides in vitro (Ref. 79). Polycationic dendrimers are colloid-sized polymeric constructs that in some instances have been shown to be biodegradable in vivo (Ref. 80) and are able to induce the so-called 'proton sponge' endo-osmotic disruption effect. Briefly, by acting as weak bases once inside the acidic endosome environment, these agents act to increase osmotic pressure across the endosomal membrane and induce swelling and

rupture of the endosome, leading to release of organelle contents. They have been employed as electrostatically associated carriers for oligonucleotides, and in vitro studies using dendrimers have shown antisense delivery and reduced luciferase expression in luciferase-expressing cell lines (Ref. 81). Further functionalised dendrimers with targeting and moieties that extend the circulatory half-life of the dendrimers (Ref. 82) indicate strong potential for dendrimers, incorporating all of the functionality of the model system in Figure 2, to overcome the barriers currently limiting extravasation and delivery of antisense in vivo. Derivatisation of polycations such as chitosan, cationic dendrimers, polyethyleneimine, and cationic poly(amino acid)s is likely to be required if the intention is to use polyelectrolyte complexes as the core of a delivery system for intravenous use. Although complexes with excess cationic charge can be used to deliver antisense therapeutics in vitro, the result of injecting such complexes intravenously is substantial uptake by the reticuloendothelial system, as well as the threat of particle aggregation following interaction with blood components. When the latter occurs, the result is usually deposition of the particles in the capillary bed of the lung. These phenomena have been well documented in the field of nonviral gene therapy – that is, using cationic polymer (Refs 83, 84, 85) or lipid complexes (Refs 86, 87, 88, 89) to deliver DNA expression plasmids. Although siRNA delivery is beyond the scope of this review, recent studies in this area (Ref. 90) suggest that small nucleic acid molecules can be delivered in neutral particles (Refs 91, 92) or as direct chemical conjugates with targeted neutral polymers (Refs 93, 94), and it is likely that similar approaches can be effective using antisense oligonucleotides. An important aspect of the use of colloidal systems to deliver antisense oligonucleotides is that the toxicity of the components of the system may be a limiting factor, as has been the case in the past with cationic liposomes.

Table 2 summarises current successes in overcoming the barriers to antisense oligonucleotide delivery to the cytoplasm of target cells, along with suggested directions for future work. At the time of writing this article, Juliano and colleagues (Ref. 75) published a



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Figure 2. Schematic representation of a colloidal particle for antisense delivery. This diagram shows an ideal construct that carries antisense oligonucleotides (protected from degradation), is able to circulate without reticuloendothelial system uptake, and has targeting, cell-penetrating and endosomal escape functionalities.

similar list of barriers to oligonucleotide delivery: there is agreement as to the problems faced – the remaining questions concern the respective solutions.

Successful antisense knockdown after systemic administration

Although the list of barriers described earlier appears imposing, antisense oligonucleotides have been shown to reduce target expression and alter disease phenotypes in many well-controlled in vivo experiments. A great number of significant publications have emerged over the past 20 years describing antisense-mediated efficacy in vivo after systemic administration

using simple injection of oligonucleotide-containing solutions. The most convincing of these combine most or all of the following properties: characterisation of the knockdown or exon skipping in vitro using robust controls [see review by Stein and Krieg (Ref. 95) for interpretation of antisense data], low doses of antisense oligonucleotide, and clear evidence of protein knockdown in vivo correlating with the observed phenotype change.

Table 3 summarises the doses used (mg/kg) and efficacy observed for selected examples of antisense efficacy in vivo across a range of target organs. It is clear that efficacy can be seen at low mg/kg doses, and that the maximum efficacy

Table 2. Barriers faced by antisense oligonucleotides when given systemically, and approaches for overcoming them^a

Barrier	Significance	Published strategies to overcome barrier	Future directions
Nuclease degradation	High	Chemical modification (Refs 26, 30, 43, 46)	None required
Renal excretion	High	Phosphorothioate modification, selection of sequences that result in high albumin-binding affinity (Refs 31, 34, 49)	Particulate strategies to avoid glomerular filtration for nonphosphorothioate
Reticuloendothelial system	High	Cholesterol conjugation (Ref. 126)	Stealth particles coated with inert polymers such as polyethyleneglycol
Extravasation	Unclear	None	Functionality to enable transcytosis across vascular endothelium
Cellular uptake	Cell-type dependent	Cell-penetrating peptides (Refs 73, 74)	Targeting functionality (antibody) to produce cell-type-specific uptake
Endosomal escape	Moderate–high	Proton-sponge endosomal escape moieties (Ref. 81)	Nontoxic endosomal escape

^aThe table is a chronological listing of the barriers faced by antisense oligonucleotides when given systemically, and approaches that may be employed to overcome these barriers. The relative importance of each barrier is rated and existing strategies to overcome the barrier identified where possible.

Table 3. Representative examples of the determination of maximal efficacy of in vivo knockdown^a

Organ	Ref.	Dose (mg/kg)	Target	% Knockdown	Chemistry	Species
Liver	101	5–50	ApoB	~90 ^b	MOE gapmer	Mouse
	72	25	EGFP	85	LNA	Mouse
Tumour	127	75	Survivin	60–80	PS	Mouse
Kidney	102	10	CTGF	83	MOE gapmer	Mouse
Skeletal muscle	5	~100 ^c	Dmd	≤30	PMO	Mouse
Heart	98	1.5	EGFR	50	PS + liposome	Rat
	99	1	B ₁ AR	30–50	PS + liposome	Rat

^aData were collected from original research articles, across a range of target organs showing doses used and the percentage decrease in expression of target mRNA or protein (% knockdown).
^bThe first reported measurement in this study was 25 days after initiation of therapy.
^cApproximate; authors used 2 mg per mouse.
 Abbreviations: ApoB, apolipoprotein B; B₁ AR, β₁ adrenoceptor; CTGF, connective tissue growth factor; Dmd, dystrophin; EGFR, epidermal growth factor receptor; EGFP, enhanced green fluorescent protein; LNA, locked nucleic acid; MOE, 2'-O-methoxyethyl; PMO, phosphorodiamidate morpholino; PS, phosphorothioate.

reported is greatest in the liver and kidney. The heart was chosen to represent tissues identified earlier in the review that show modest levels of tissue drug concentration. Although many groups including ourselves (Refs 96, 97) have shown antisense efficacy in the myocardium, the ceiling on the maximum possible level of target suppression appears to be around 50%, even when delivery strategies such as liposome encapsulation are used (Refs 98, 99). Similarly, correction of aberrant splicing in skeletal muscle has required large doses of antisense to produce relatively low levels of correction (Refs 5, 100), although this may be enough to cause phenotypic improvement, and in these impressive studies many muscle fibres show evidence of correction. Correction of aberrant splicing in the liver by the same investigators was more successful, with 85% correction (Ref. 72) at lower doses than used in skeletal muscle. Maximum levels of knockdown in cardiac and skeletal muscle therefore appear to be lower than that for the liver, in which up to 90% silencing has been shown in vivo (e.g. Ref. 101), and the kidney, in which 83% knockdown in the proximal tubules has been shown (Ref. 102). Thus, the literature appears to suggest that significant enhancement of tissue and cellular uptake using delivery systems is required for high-efficacy silencing in tissues such as the heart and skeletal muscle.

While a comprehensive coverage of successful employment of antisense oligonucleotides as research tools is beyond the scope of this review, it is pertinent to consider some key examples of convincing in vivo data in which the experimental controls were rigorous and the efficacy noteworthy. We direct the reader to examples of local or systemic injections of a range of antisense oligonucleotides (PS, OMe and MOE gapmers, PMO oligonucleotides and LNA antisense) which were shown to produce specific target mRNA knockdown (or exon skipping) (see Refs 51, 96, 100, 101, 103, 104, 105, 106, 107, 108, 109, 110, 111, 112) in a range of tissues (liver, gastrointestinal tract, brain, skeletal muscle, vasculature) (see Refs 51, 96, 101, 103, 104, 107, 110) and against a range of targets (enzymes, intracellular signaling molecules) (see Refs 9, 104, 107, 108, 112) in order to reverse disease phenotype.

Outstanding examples of impressive antisense effects in vivo using simple injection not surprisingly relate to organs with naturally

leaky vascular beds – in particular the liver and in tumours (Ref. 113). Apolipoprotein B knockdown has been reported in carefully controlled studies in animals (Ref. 101) and in dyslipidaemic humans (Ref. 114) using moderately low doses of ISIS antisense oligonucleotides, and the future of this strategy appears to be promising. Tumour regression and inhibition of metastasis by targeting a kinase suppressor of Ras (Ref. 113) has been elegantly demonstrated – a case in which specific intracellular signalling molecules are critical for tumour development and where gene-silencing approaches may be more useful than traditional small-molecule strategies. Conferring of positive charge on PNAs, using lysine (K) residues at the C-terminus, greatly improves the drug distribution to a range of tissues after intraperitoneal injection (Ref. 51). In this study, ‘PNA-4K’ antisense oligonucleotides demonstrated efficacies (correction of aberrant splicing in this case) equal to or greater than MOE antisense oligonucleotides in a range of organs, whereas uncharged PNA or PMO antisense oligonucleotides were relatively ineffective.

Direct measurement of in vitro target mRNA knockdown (or exon skipping) and/or subsequent target protein knockdown is often not possible in humans due to the inability to excise and collect target tissues for measurement of mRNA levels. As a result, reversal of disease phenotype is often the only measure of antisense drug efficacy and this is, at best, only an indirect measure of target mRNA knockdown. This is demonstrated by the first antisense drug to reach the market, fomivirsen, for which clear evidence of clinical efficacy (Refs 115, 116) but no direct evidence of antisense-mediated target knockdown in humans can be found in the literature. Furthermore, only a limited number of antisense-oligonucleotide-based therapeutics have entered clinical trials, with the vast majority being of PS chemistry and with most studies reported being Phase I trials in which safety, rather than efficacy, was the primary endpoint (Refs 34, 117, 118, 119, 120, 121, 122, 123). Later-phase studies with a PS oligonucleotide targeting BCL2 mRNA returned promising results as a cancer therapy adjuvant in humans (Refs 124, 125); however, these studies did not directly measure target mRNA

or protein knockdown. One excellent example of antisense target knockdown with a MOE gapmer antisense oligonucleotide was reported by Kastelein and colleagues (Ref. 1). Following on from animal studies (Ref. 101; discussed earlier in this section), these workers reported that simple intravenous administration of an antisense oligonucleotide targeting apolipoprotein B mRNA in humans produced dose-dependent reductions in circulating apolipoprotein B protein levels and LDL-cholesterol levels. Although not a direct measure of antisense target mRNA knockdown, the ability to measure changes in circulating levels of apolipoprotein B protein, and the clear dose-dependency of the protein knockdown and phenotype changes (reduced LDL-cholesterol) in this study provide convincing evidence of successful antisense targeted apolipoprotein B mRNA knockdown.

Conclusions and outstanding research questions

The large body of literature describing successful antisense use in vivo is ample evidence that this method of gene silencing is robust and reproducible. The antisense platform has enjoyed a considerable 'head-start' on other gene-silencing strategies such as those employing RNA interference. Lessons learnt from this period, in addition to those from extensive development of siRNA agents as therapeutics, provide great hope that antisense drugs will emerge in the near term. In several cases, the nature and location of the target cell type and target gene product will allow the use of simple injection of antisense oligonucleotides as potent and safe therapeutic agents; this may well be the case for ISIS 301012. For the liver, renal proximal tubules and the spleen, simple systemic administration may be sufficient to produce safe and effective therapeutic gene silencing. Where other cell types are targeted, delivery systems that overcome the 'trapping' of oligonucleotide within the liver, kidney and spleen and resultant low tissue concentrations are very likely to improve therapeutic indices. While in some instances this has already been achieved using liposomal delivery, endosomal escape agents, and targeting moieties, a step-change in antisense oligonucleotide therapeutics calls for further progress in antisense delivery systems.

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Further reading, resources and contacts

Publications

Crooke, S., ed. (2008) *Antisense Drug Technology; Principles, Strategies and Applications*, CRC Press, Boca Raton, FL, USA

This book provides a comprehensive review of the development of antisense oligonucleotides as therapeutic agents. The chapter authors are from ISIS pharmaceuticals, which perhaps limits the discussion of antisense oligonucleotide chemistries other than MOE, but this book remains indispensable to those in the field of antisense therapeutics.

Rayburn, E.R. and Zhang, R. (2008) Antisense, RNAi, and gene silencing strategies for therapy: mission possible or impossible? *Drug Discovery Today* 13, 513-521

This article includes an up-to-date listing of past and current clinical trials using antisense oligonucleotides.

Juliano, R. et al. (2008) Mechanisms and strategies for effective delivery of antisense and siRNA oligonucleotides. *Nucleic Acids Research* 36, 4158-4171

This review provides an insightful look at overcoming the barriers to silencing for both single- and double-stranded oligonucleotides, from a group with extensive experience in the field.

Websites

The RNAi.net website contains breaking news stories, job vacancies, product information and conference information in the field of RNAi:

<http://www.rnai.net/>

Features associated with this article

Figures

Figure 1. Fates of antisense oligonucleotides following systemic administration.

Figure 2. Schematic representation of a colloidal particle for antisense delivery.

Tables

Table 1. Tissue distribution of the major classes of modified antisense oligonucleotides after systemic administration.

Table 2. Barriers faced by antisense oligonucleotides when given systemically, and approaches for overcoming them.

Table 3. Representative examples of the determination of maximal efficacy of in vivo knockdown.

Citation details for this article

Paul J. White, Frank Anastasopoulos, Colin W. Pouton and Ben J. Boyd (2009) Overcoming biological barriers to in vivo efficacy of antisense oligonucleotides. *Expert Rev. Mol. Med.* Vol. 11, e10, March 2009, doi:10.1017/S1462399409001021